

A Novel Controlled-Release Formulation of Quetiapine for Extended Antipsychotic Action

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ABSTRACT

In the current study, several grades of HPMC and ethyl cellulose were used as the retarding polymers to create controlled release tablets of quetiapine fumarate. All the formulations were created utilizing the direct compression method on an eight-station rotary tablet punching machine with a 12mm punch. All the formulations combined demonstrated good flow characteristics in terms of angle of repose, bulk density, and tapped density. The created tablets had good post-compression properties, and they met all the I.P.-required quality control evaluation criteria. F2 is regarded as an optimal formulation because it had the highest percentage of drug release of all the formulations (97.3 percent in 8 hours). As the polymer content increased, the formulations incorporating HPMC K100M displayed greater retardation. Guar gum compositions failed to generate the desired drug release pattern.

KEYWORDS: Quetiapine fumarate, HPMC K15M, HPMC K100M, Guar gum, Controlled release tablets.

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INTRODUCTION

The goal of any drug delivery system is to provide a therapeutic amount of drug in the proper site in the body to achieve promptly and then maintain the desired drug concentration. That is, the drug delivery system should deliver a drug at a rate dictated by the needs of the body over a specified period of treatment.

1.1.1. Oral drug delivery:

This is the most widely utilized route of administration among all the routes that have been explored for systemic delivery of drugs via pharmaceutical products of different dosage forms. The oral route is considered the most natural, uncomplicated, convenient, and safe due to its ease of administration, patient acceptance, and cost-effective manufacturing process. Oral drug delivery is the most desirable and preferred method of administering therapeutic agents for their systemic effects. In addition, oral medication is generally considered the first avenue investigated in the discovery and development of new drug entities, and pharmaceutical formulations, mainly because of patient acceptance and convenience in administration. The oral route of drug administration has wide acceptance up to 50-60% of total dosage forms. Solid dosage forms are popular because of ease of administration, accurate dosage, self-medication, pain avoidance, and most importantly patient compliance. The most popular solid dosage forms are tablets and capsules. But the important drawback of these dosage forms is the difficulty to swallow. The oral dosage form is the most popular route for drug therapy. Over 80% of the drugs formulated to produce systemic effects in the United States are produced in oral dosage forms. Compared to other oral dosage forms, tablets are the manufacturer's dosage form of choice because of their relatively low cost of manufacture and package. The term modified-release drug product is used to describe products that alter the timing and/or the rate of release of the drug substance. A modified-release dosage form is defined "as one for which the drug-release characteristics of time course and/or location are chosen to accomplish therapeutically or convenience objectives not offered by conventional dosage forms such as solutions, ointments, or promptly dissolving dosage forms as presently recognized".¹⁻³

Controlled release drug delivery system:

The US FDA defines a sustained release dosage form is one that allows a reduction in dosing frequency from that necessitated by a conventional dosage form, such as a solution or an immediate release dosage form.⁴

Drug Candidates for Controlled Release Products

To be a successful sustained release product the drug must be released from the dosage form at a predetermined rate, dissolve in gastrointestinal fluids, maintain gastrointestinal residence time, and be absorbed at a rate that will replace the amount of drug being metabolized and excreted.⁵⁻⁶

Characteristics of Controlled release products.

They exhibit neither very slow nor very fast rates of absorption and excretion. They are uniformly absorbed from the gastrointestinal tract. They are administered in relatively small dosages. They possess a good margin of safety. They are used in the treatment of chronic rather than acute conditions. 6-8

Advantages of Controlled release dosage forms over conventional dosage forms:

Less fluctuation in drug blood levels. Reduction in dosing frequency, Enhanced convenience, and compliance, Reduction in adverse side effects, and Reduction in overall healthcare cost.

Disadvantages: Loss of flexibility in adjusting the drug dose and/or dosage regimen and risk of sudden and total drug release or dose dumping due to a failure of technology. Sustained release products contain a higher drug load and thus any loss of integrity of the release characteristics of the dosage form has potential problems. They should be never crushed or chewed, as the slow-release characteristics may be lost, and toxicity may result. This is particularly important in patients unable to follow whole tablets, a problem commonly affecting the elderly. The large size of the Sustained release product may cause difficulties in ingestion or transit to the gut. 9-11

Controlled Release Technology for Oral Dosage Form.

For orally administered dosage forms, sustained release action is achieved by affecting the rate at which drugs are released from the dosage form and or by slowing the transit time of the dosage form through the gastrointestinal tract. The rate of drug release from solid dosage forms may be modified by the technologies which in general are based on: Modifying drug dissolution by controlling access of biological fluids to the drug using barrier coatings. Controlling drug diffusion rates from dosage forms. Chemical reaction or interaction between the drug substance or its pharmaceutical barrier and site-specific biological fluids.

Monolithic Matrix System: In pharmaceutical CRDDS, matrix-based systems are the most used type of release controlling methodology owing to their simple manufacturing process. The preparation of a tablet with the matrix involves the direct compression of the blends of drug, release retardant and other additives, in which the drug is uniformly distributed throughout the matrix core of the release retardant. Alternatively, drug-release retardant blends may be granulated to make the mix suitable for the preparation of tablets by wet granulation or beads. 12-14

Based on the chemical nature of the release retardant(s), the matrix systems are classified as given in Table 1.

Table No 1.1: Classification of Matrix Systems. 15-18

Type of the Matrix System	Mechanism
Hydrophilic	Unlimited swelling delivery by diffusion, Limited swelling-controlled delivery eg.: Hydroxyethyl cellulose, Hydroxypropyl methylcellulose.
Inert	Inert nature Controlled delivery by diffusion eg.: Ethyl cellulose
Lipidic	Delivery by diffusion & erosion eg.: Carnauba wax.
Biodegradable	Nonlipidic nature Controlled delivery by surface erosion
Resin Matrices	Drug release from drug-resin complex eg.: Ion exchange resins

Mechanism of Drug Release from Matrix Tablets

As shown in Figure 1, in erodible matrices, polymer erosion from the surface of the matrix determines the drug release; whilst in hydrophilic matrices, formation of the gel layer and its dynamics as a function of time determines the drug release. Gel layer thickness, which determines the diffusion path length of the drug, corresponds to the distance between the diffusion and erosion fronts. As the swelling process proceeds, the gel layer gradually becomes thicker, resulting in progressively slower drug release rates; however, due to continuous hydration, polymer disentanglement occurs from the surface of the matrix, resulting in a gradually decreasing depletion zone and an increased dissolution rate. 19-21

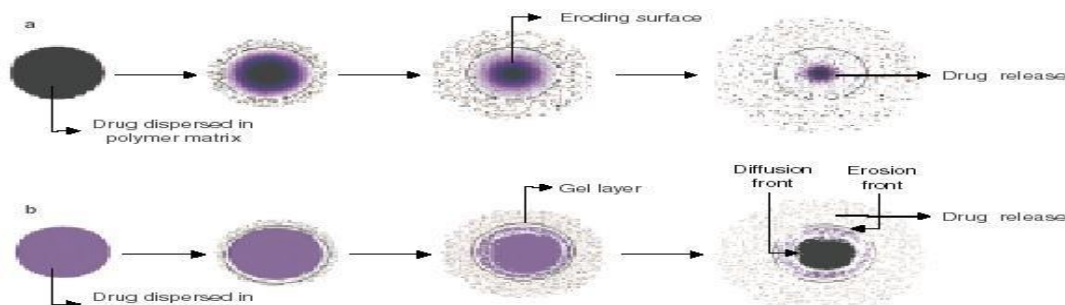
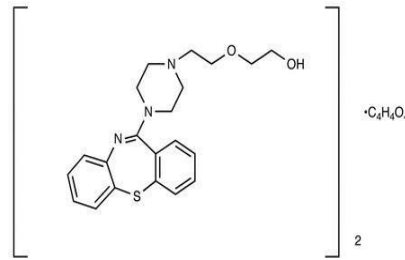


Fig.1.1. Schematic drug release from matrix diffusion controlled-release drug delivery systems with the drug homogeneously dispersed in: (a) an erodible polymer matrix; and (b) a hydrophilic, swellable polymer matrix.

DRUGPROFILE22-26

Drug : Quetiapine fumarate
 Solubility : moderately soluble in water 3.29mg/ml Soluble in DMSO (36mg/ml), water (<1mg/ml), and ethanol (<1mg/ml)
 Physical state: Solid Melting point: 174-176°C (lit.) CAS NO : 11974-72-2
 Structure:



Molecular formula: $2(C_{21}H_{25}N_3O_2S) \cdot C_4H_4O_4$
 Molecular weight: Average: 383.507 Monoisotopic: 383.166747749
 Bioavailability : 100%.
 Half-life : 6 hours
 Protein binding : 83%
 Dose : 25-400mg
 Category : Antipsychotic Agents

METHODOLOGY

Determination of UV Absorption maxima:

Quetiapine fumarate solution was prepared in 0.1 N HCL and diluted suitably. The UV spectrum of the solution was taken on Lab India 3200 UV/Vis double beam Spectrophotometer. The Solution exhibited UV maxima at 298 nm. The procedure was repeated with pH 6.8 phosphate buffer.

Preparation of Standard Calibration Curve of Quetiapine fumarate:

100 mg of Quetiapine fumarate was accurately weighed and dissolved in little amount of Methanol and make up the final volume up to 100 ml with 0.1 N HCl (pH 1.2) to prepare stock solution. The 10 ml of stock solution was further diluted with 0.1 N HCl (pH 1.2) in 100ml to get 100µg/ml (working standard). Then 0.2, 0.4, 0.6, 0.8, and 1 ml of working standard was taken in 10 ml standard volumetric flask and made up the volume with 0.1 N HCl to prepare 2µg, 4µg, 6µg, 8µg, and 10µg drug per ml solution. Then the absorbance was measured in a UV spectrophotometer at 298 nm against 0.1 N HCl (pH 1.2) as blank. The absorbance so obtained was tabulated as in Table 2.1.1 Calibration curve was constructed and shown in Fig. 2.1.2 The procedure was repeated with pH 6.8 phosphate buffer and absorbance's were measured at 299nm. The absorbance and standard graph were mentioned in Table 2.1.1 and figure 2.1.2 respectively. 27,28

Tablet formulation:

Formulation of Quetiapine fumarate Controlled release Tablet by Direct-Compression:

Composition of preliminary trials for Quetiapine fumarate Controlled release Tablet by direct compression is shown in table 6.1. All the ingredients were weighed. required quantity of drug and excipient mixed thoroughly in a polybag. The blend is compressed using rotary tablet machine-8 station with 12mm flat punch, B tooling. Each tablet contains 100mg of Quetiapine fumarate and other pharmaceutical ingredients.

2.1.1 Formulation of Quetiapine fumarate Controlled release tablets

INGREDIENT	F1	F2	F3	F4	F5	F6
Quetiapine fumarate	100	100	100	100	100	100
HPMCK15M	50	150	-	-	-	-
HPMC K100M	-	-	50	100	-	-
GUARGUM	-	-	-	-	50	200
Talc	5	5	5	5	5	5
Mg.Stearate	5	5	5	5	5	5

MCCpH102	Q. S	Q. S	Q. S	Q. S	Q. S	Q. S
TOTAL	500	500	500	500	500	500

All ingredients are expressed in mg only

Evaluation parameters:

Precompression parameters:

Bulk Density (Db):

It is the ratio of total mass of powder to the bulk volume of powder. It was measured by pouring the weight powder (passed through standard sieve #20) into a measuring cylinder and initial weight was noted. This initial volume is called the bulk volume. From this the bulk density is calculated according to the formula mentioned below. It is expressed in g/ml and is given by,

$$D_b = M / V_b$$

Where, M is the mass of powder

V_b is the bulk volume of the powder.

Tapped Density (Dt):

It is the ratio of total mass of the powder to the tapped volume of the powder. Volume was measured by tapping the powder for 750 times and the tapped volume was noted if the difference between these two volumes is less than 2%. If it is more than 2%, tapping is continued for 1250 times and tapped volume was noted. Tapping was continued until the difference between successive volumes is less than 2% (in a bulk density apparatus). It is expressed in g/ml and is given by,

$$D_t = M / V_t$$

Where,

M is the mass of powder

V_t is the tapped volume of the powder.

1. Angle of Repose (Θ):

The friction forces in a loose powder can be measured by the angle of repose (q). It is an indicative of the flow properties of the powder. It is defined as maximum angle possible between the surface of the pile of powder and the horizontal plane

$$\tan(\Theta) = h / r$$

$$\Theta = \tan^{-1}(h / r)$$

Where,

Θ is the angle of repose. h is the height in cm

r is the radius in cm

The powder mixture was allowed to flow through the funnel fixed to a stand at definite height (h). The angle of repose was then calculated by measuring the height and radius of the heap of powder formed. Care was taken to see that the powder particles slip and roll over each other through the sides of the funnel. Relationship between angle of repose and powder flow property.

Angle of Repose as an Indication of Powder Flow Properties

Shown in table no 2.1.2:

Sr.No.	Angle of Repose (°)	Type of Flow
1	<20	Excellent
2	20-30	Good
3	30-34	Passable
4	>34	Very Poor

Carr's index (or) % compressibility:

$$I = \frac{D_t - D_b}{D_t} \times 100$$

It indicates powder flow properties. It is expressed in percentage and is given by,

Where,

D_t is the tapped density of the powder and D_b is the bulk density of the powder.

Relationship between % compressibility and flowability

Shown in table no 2.1.3

Srno.	% Compressibility	Flow ability
1	5-12	Excellent
2	12-16	Good
3	18-21	Fair/Passable
4	23-35	Poor
5	33-38	Very Poor
6	<40	Very Very Poor

Hausner ratio: Hausner ratio is an indirect index of ease of powder flow. It is calculated by the following formula.

$$\text{Hausner ratio} = \frac{D_t}{D_b}$$

Where, D_t is the tapped density, D_b is the bulk density.

Lower Hausner ratio (<1.25) indicates better flow properties than higher ones (>1.25).

Postcompression parameters:

Weight variation:

20 tablets were selected randomly from the lot and weighed individually to check for weight variation. Weight variation specification as per I.P. is shown in table No. 2.1.4

Weight Variation Specification as per IP

Average Weight of Tablets	% Deviation
80 mg or less	±10
More than 80 mg but less than 250 mg	±7.5
250 mg or more	±5

Hardness:

Hardness or tablet crushing strength (f_c), the force required to break a tablet in a diametric compression was measured using Monsanto tablet hardness tester. It is expressed in kg/cm².

Thickness:

Three tablets were selected randomly from each batch and thickness was measured by using Vernier Caliper.

Friability (F):

Friability of the tablet determined using Roche friabilator. This device subjects the tablet to the combined effect of abrasion and shock in a plastic chamber revolving at 25 rpm and dropping a tablet at the height of 6 inches in each revolution. Pre weighed sample of tablets was placed in the friabilator and were subjected to the 100 revolutions. Tablets were dusted using a soft muslin cloth and reweighed. The friability (F) is given by the formula. 29-31

$$F = \frac{W_{\text{initial}} - W_{\text{final}}}{W_{\text{initial}}} \times 100$$

In-Vitro drug release:

In vitro dissolution studies were carried out by using 900 ml of 0.1N HCl in USP dissolution apparatus by using paddle method for about 2 hours. After 2 hours the dissolution medium was withdrawn keeping the tablet in the dissolution basket. Then pH 6.8 phosphate buffer was added to the dissolution medium (900 ml) and the dissolution was carried out for about 6 hours. The samples were withdrawn at regular time intervals of 30 min, 1 hour, 2 hr, 3, 5, 6, 7 & 8 hours respectively. 32, 33

Assay:

10 tablets were weighed and triturated. The tablet triturate equivalent to 10 mg of the drug was weighed accurately, dissolved in pH 1.2 buffer, and diluted to 100 ml with the same. Further dilutions were done suitably to get a concentration of 10 µg/ml with simulated gastric fluid pH 1.2. Absorbance was read at 210 nm against the reagent blank, and the concentrations of Quetiapine fumarate in µg/ml was determined by using the regression equation. 11-15

$$Y = 0.007x + 0.001$$

Drug content in mg/tablet = conc. µg/ml * dilution factor

% Drug content = drug content in mg * 100 / label claim.

RESULTS & DISCUSSION

Standard Calibration curve of Quetiapine fumarate:

Table 2.1.5: Concentration and absorbance obtained for calibration curve of Quetiapine fumarate in 0.1 N hydrochloric acid buffer (pH 1.2)

S.No.	Concentration (µg/ml)	Absorbance* (at 298 nm)
1	2	0.193
2	4	0.34
3	6	0.461
4	8	0.579
5	10	0.709
Correlation Coefficient = 0.9985 y = 0.0636x + 0.0751		

It was found that the estimation of Quetiapine fumarate by UV spectrophotometric method at λ_{max} 298 nm in 0.1N Hydrochloric acid had good reproducibility and this method was used in the study. The correlation coefficient for the standard curve was found to be close to 1, at the concentration range, 2-10 µg/ml. The regression equation generated was $y = 0.0636x + 0.0751$.

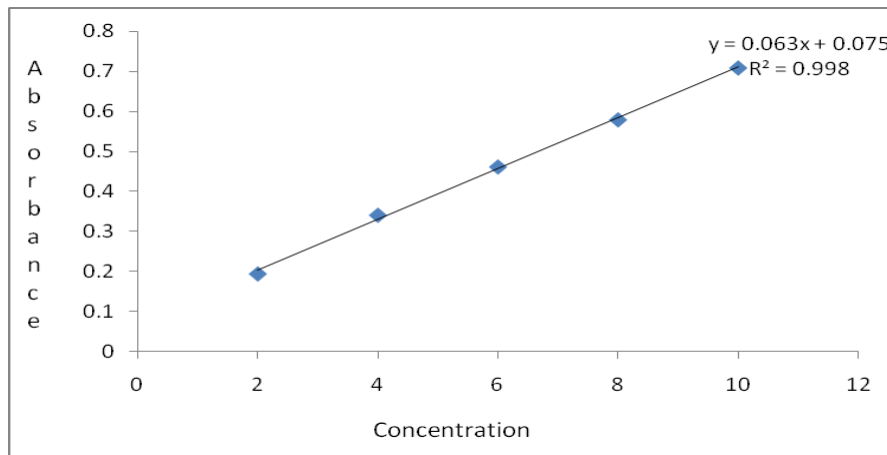


Fig 1.1.2: Standard graph of Quetiapine fumarate in 0.1N HCl

Table 1.2.5: Concentration and absorbance obtained for calibration curve of Quetiapine fumarate in pH 6.8 Phosphate buffer.

S.No.	Concentration (µg/ml)	Absorbance* (at 299 nm)
1	2	0.193
2	4	0.331
3	6	0.446
4	8	0.553
5	10	0.677
Correlation Coefficient = 0.9982 y = 0.0595x + 0.083		

It was found that the estimation of Quetiapine fumarate by UV spectrophotometric method at λ_{max} 299 nm in pH 6.8 Phosphate buffer had good reproducibility and this method was used in the study. The correlation coefficient for the standard curve was found to be close to 1, at the concentration range, 2-10 µg/ml. The regression equation generated was $y = 0.0595x + 0.083$.

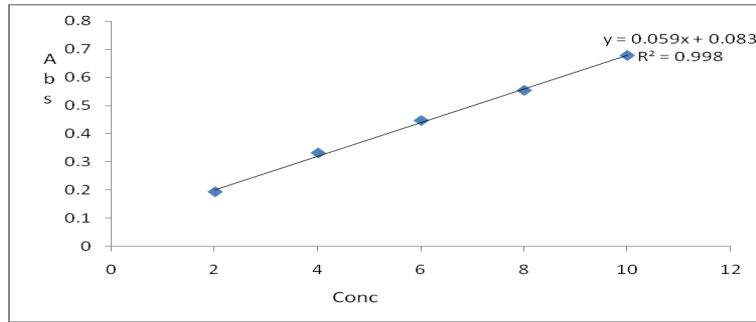


Fig1.1.3:Standard graph of Quetiapine fumarate in pH 6.8 Phosphate buffer

Evaluation Parameters for Controlled release tablets of Quetiapine fumarate:

Pre-compression parameters:

The data were shown in Table 7.3. The values for angle of repose were found in the range of 25°-30°. Bulk densities and tapped densities of various formulations were found to be in the range of 0.41 to 0.50 (gm/cc) and 0.50 to 0.58 (gm/cc) respectively. Carr's index of the prepared blends falls in the range of 13.06% to 18.18%. The Hausner ratio falls in the range of 1.14 to 1.22. From the result it was concluded that the powder blends had good flow properties, and these can be used for tablet manufacture.

Table 1.2.6: Pre-compression parameters

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Formulations	Bulk Density (gm/cm ²)	Tap Density (gm/cm ²)	Carr's Index (%)	Hausner ratio	Angle Of Repose (Θ)
F1	0.45	0.55	18.18	1.22	27.91
F2	0.50	0.58	13.79	1.16	29.34
F3	0.50	0.58	13.79	1.16	29.34
F4	0.47	0.55	14.54	1.17	28.23
F5	0.41	0.50	18	1.21	26.78
F6	0.41	0.54	18.11	1.22	26.71

Post-compression parameters:

Weight variation test:

Tablets of each batch were subjected to weight variation test, difference in weight and percent deviation was calculated for each tablet and was shown in the Table 1.2.7. The average weight of the tablet is approximately in the range of 495 to 505 mg, so the permissible limit is ±5% (>220 mg). The results of the test showed that, the tablet weights were within the pharmacopoeia limit.

Hardness test:

Hardness of the three tablets of each batch was checked by using Pfizer hardness tester and the data were shown in Table 1.2.8. The results showed that the hardness of the tablets is in the range of 4 to 4.5 kg/cm², which was within IP limits.

Thickness:

Thickness of three tablets of each batch was checked by using Vernier Caliper and data shown in Table 1.2.9. The result showed that thickness of the tablet is ranging from 5.00 to 6.14 mm.

Friability:

Tablets of each batch were evaluated for percentage friability and the data were shown in the Table 1.3.0. The average friability of all the formulations lies in the range of 0.30 to 0.51% which was less than 1% as per official requirement of IP indicating a good mechanical resistance of tablets.

1.2.7. Post-Compression parameters:

1.2.7. Post-Compression parameters:					
FD	Weight variation (mg)	Hardness (kg/cm ²)	Thickness (mm)	Friability (%)	Assay (%)
F1	494	4.5	5.5	0.43	97.23

F2	510	4.2	5.5	0.49	98.16
F3	502	4.3	5.5	0.49	98.16
F4	508	4.3	5.5	0.34	98.55
F5	506	4.4	5.5	0.34	99.25
F6	504	4.5	5.5	0.43	98.5

Assay: Assay studies were performed for the prepared formulations. From the assay studies it was concluded that all the formulations were showing the % drug content values within 97.23-99.25%.

In vitro Dissolution studies:

In vitro dissolution studies were carried out by using 900ml of 0.1 N HCl in USP dissolution apparatus by using paddle method for about 2 hours. After 2 hours the dissolution medium was withdrawn keeping the tablet in the dissolution basket. Then pH 6.8 phosphate buffer was added to the dissolution medium (900ml) and the dissolution was carried out for about 6 hours. The samples were withdrawn at regular time intervals of 30 min, 1 hour, 2 hr, 3, 5, 6, 7 & 8 hours respectively. The results were displayed in table 1.2.8.

Table 1.2.8: In vitro dissolution data

Time(Hrs)	F1	F2	F3	F4	F5	F6
0.5	25.5	16.4	15.4	10.4	49.5	18.9
1	46.7	26.7	29.4	16.5	78.8	28.3
2	76.5	34.6	38.5	28.6	96.9	36.4
3	98.4	42.4	55.4	39.5	96.1	49.5
4		55.4	68.4	48.5		69.3
5		67.4	87.1	59.4		78.1
6		85.4	98.3	69.2		89.7
7		91.5	82.3	74.5		97.5
8		97.3				

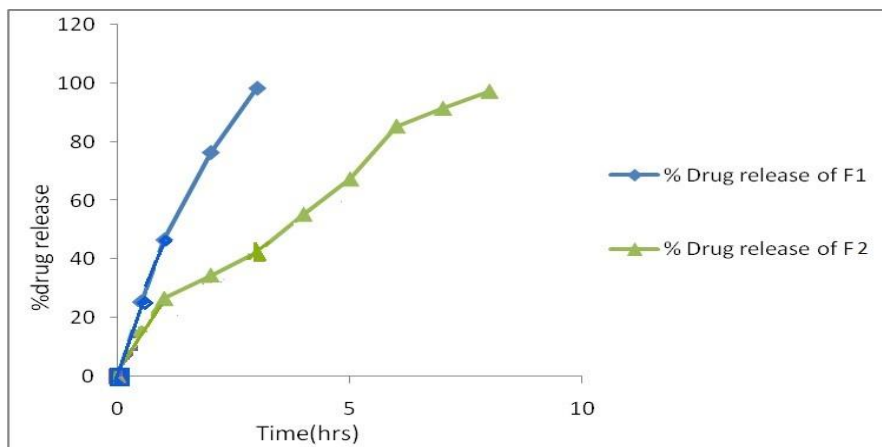


Fig 1.1.4: Dissolution profile of formulations prepared with HPMC K15M polym

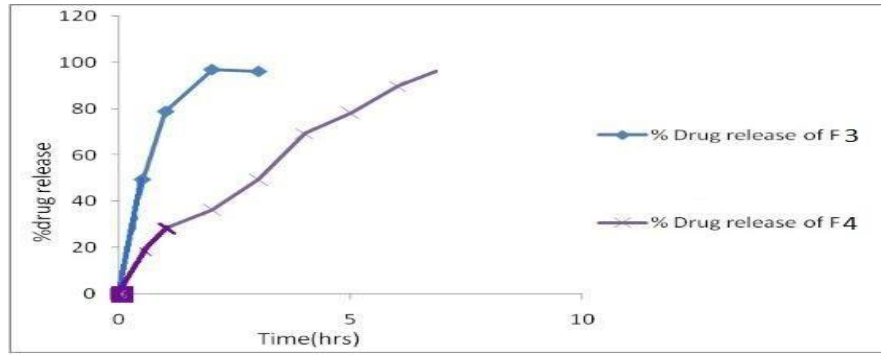


Fig1.1.5:Dissolutionprofileof formulationspreparedwith HPMC K100Mpolymer

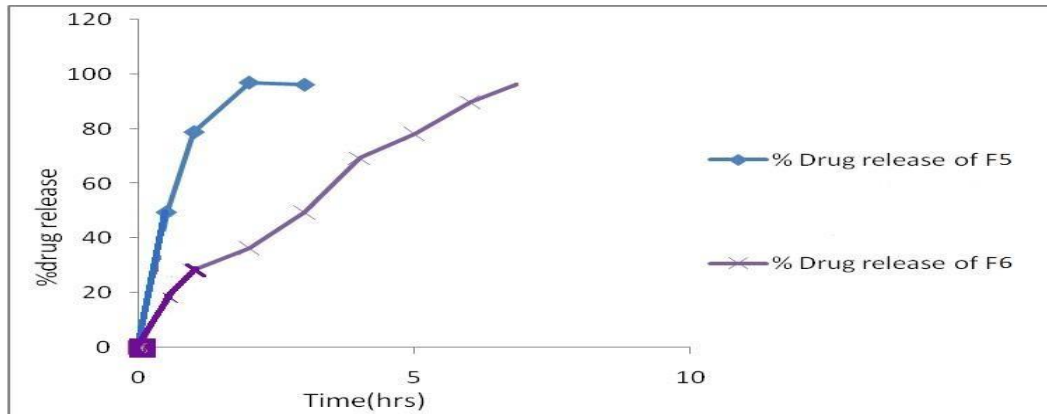


Fig1.1.6:DissolutionprofileofformulationspreparedwithGuar gum aspolymer

From the tabular column 7.5 it was evident that the formulations prepared with HPMCK15Masretardingpolymerinlowconcentrationthepolymerwasunabletoproducetherequiredretardingactiontothetablets. As the concentration of polymer increases the retarding nature was also increased. HPMC K15 M in the concentration of 150 mg showed good % drug release i.e., 97.3 in 8 hours.

Whereas in case of formulations prepared with HPMC K100 M as retarding polymer, the formulations with 50 mg concentration of polymer showed complete drug release in 6 hours only, whereas the concentration of polymer increases the retarding nature also increased. The Formulation Containing HPMC K100M in 100 Mg Concentration Showed good retarding nature with required drug release in 8 hours i.e., 82.3%.

Whereas in case formulations prepared with Guar gum as retarding polymer, as the concentration of polymer increases the retarding nature was also increased. When compared with HPMC polymers it was failed to produce desired drug release pattern.

From the above results it was evident that the formulation F2 is best formulation with desired drug release pattern extended up to 8 hours.

Application of Release Rate Kinetics to Dissolution Data:

Various models were tested for explaining the kinetics of drug release. To analyze the mechanism of the drug release rate kinetics of the dosage form, the obtained data were fitted into zero-order, first order, Higuchi, and Korsmeyer-Peppas release model.

Table 1.2.9: Release kinetics data for optimised formulation

CUMULATIVE (% RELEASE) Q	TIME (T)	ROOT (T)	LOG(% RELEASE)	LOG(T)	LOG(% REMAIN)	RELEASE RATE (CUMULATIVE % RELEASE/t)	1/CUM % RELEASE	PEPPAS log Q/100	% Drug Remaining	Q01/3	Qt1/3	Q01/3-Qt1/3
0	0	0			2.000				100	4.642	4.64	0.00
9.89											2	0
16.76	0.5	0.707	0.995	-0.301	1.955	19.780	0.1011	-1.005	90.11	4.642	4.48	0.15
											3	8

22.53	1	1.000	1.224	0.000	1.920	16.760	0.0597	-0.776	83.24	4.642	4.36	0.27
27.43											6	5
33.66	2	1.414	1.353	0.301	1.889	11.265	0.0444	-0.647	77.47	4.642	4.26	0.37
37.11											3	9
44.67	3	1.732	1.438	0.477	1.861	9.143	0.0365	-0.562	72.57	4.642	4.17	0.47
53.87											1	0
61.3	4	2.000	1.527	0.602	1.822	8.415	0.0297	-0.473	66.34	4.642	4.04	0.59
69.1											8	3
78.2	5	2.236	1.569	0.699	1.799	7.422	0.0269	-0.431	62.89	4.642	3.97	0.66
84.22											7	5
90.33	6	2.449	1.650	0.778	1.743	7.445	0.0224	-0.350	55.33	4.642	3.81	0.83
											1	1
	7	2.646	1.731	0.845	1.664	7.696	0.0186	-0.269	46.13	4.642	3.58	1.05
											6	5
	8	2.828	1.787	0.903	1.588	7.663	0.0163	-0.213	38.7	4.642	3.38	1.25
											2	9
	9	3.000	1.839	0.954	1.490	7.678	0.0145	-0.161	30.9	4.642	3.13	1.50
											8	4
	10	3.162	1.893	1.000	1.338	7.820	0.0128	-0.107	21.8	4.642	2.79	1.84
											4	8
	11	3.317	1.925	1.041	1.198	7.656	0.0119	-0.075	15.78	4.642	2.50	2.13
											8	3
	12	3.464	1.956	1.079	0.985	7.528	0.0111	-0.044	9.67	4.642	2.13	2.51
											0	1

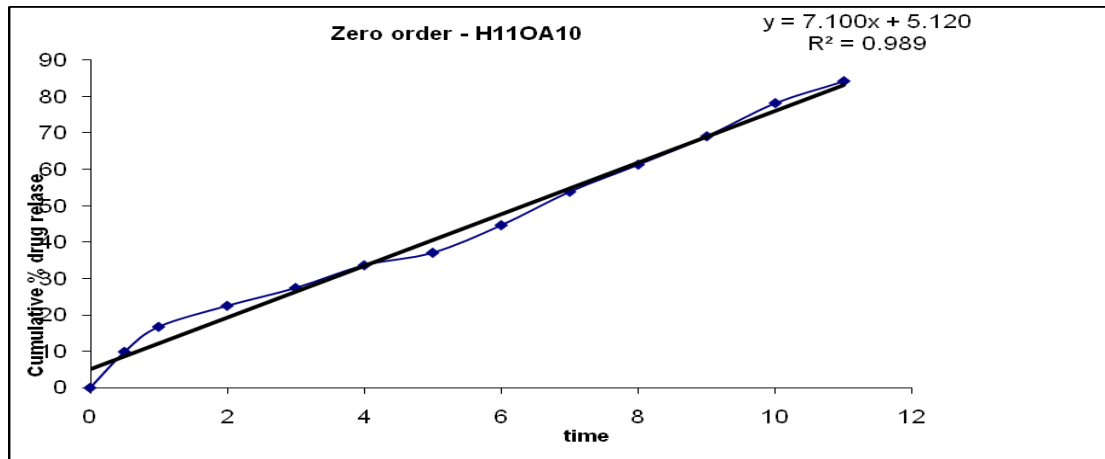


Fig1.1.7:Zeroorderreleasekineticsgraph

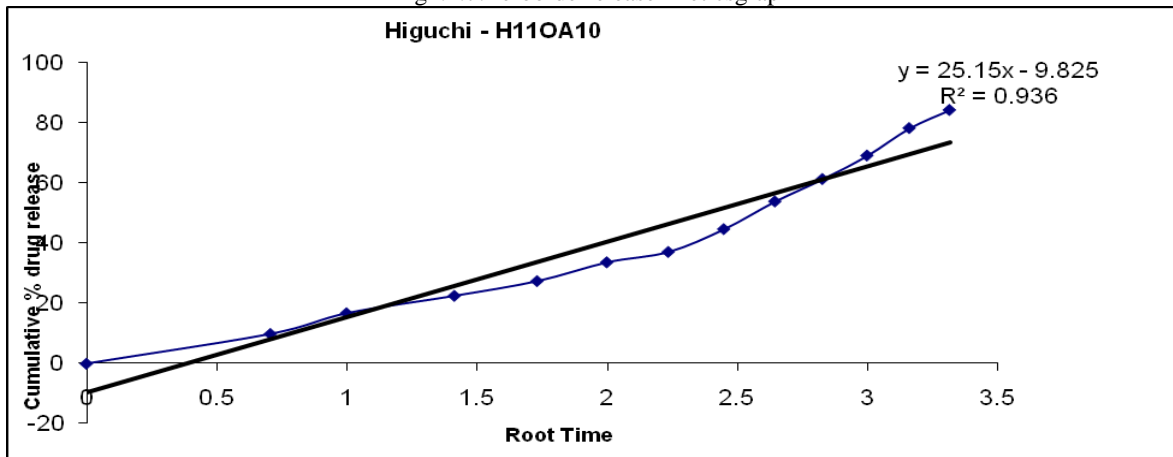


Fig1.1.8:Higuchireleasekineticsgraph

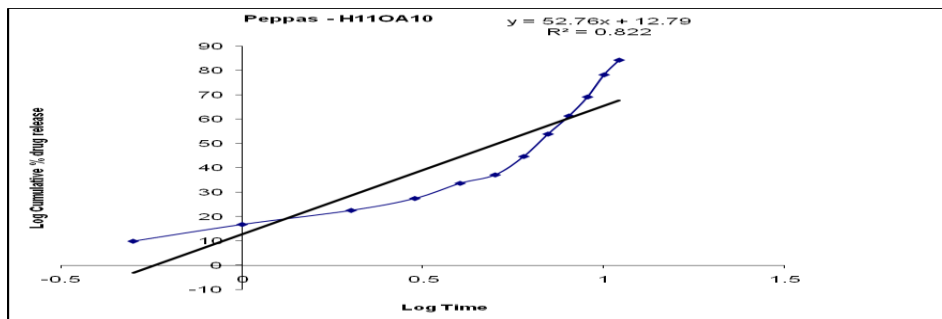


Fig1.1.9:Kars mayerpeppasgraph

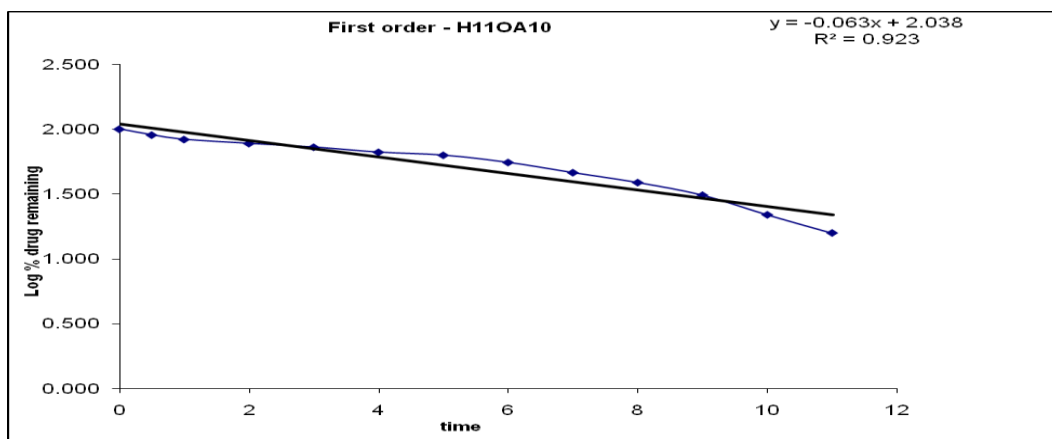


Fig 1.2.0:Firstorderrelease kineticsgraph

From the above graphs it was evident that the formulation F2 was followed Zero order release mechanism.

CONCLUSION

By using various grades of HPMC and ethyl cellulose as the retarding polymers, an effort has been made in the current study to create controlled release tablets of quetiapine fumarate. On an eight-station rotary tablet punching machine, a 12mm punch was used to prepare all the formulations utilizing the direct compression method. The combination of all the formulations displayed favorable flow characteristics in terms of angle of repose, bulk density, and tapped density. The produced tablets displayed favorable post-compression properties and passed all the quality control assessment criteria in accordance with I.P. limitations. The F2 formulation, which showed the highest percentage of drug release of 97.3 percent in 8 hours among all the formulations, is regarded as an optimal formulation. As the polymer content increased, the formulations incorporating HPMC K100M displayed greater retardation. Guar gum-based formulations failed to provide the anticipated medication release pattern.

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Conflict of interest: NONE

REFERENCES

1. Ansel H., Allen L. & Jr. Popovich N. Ansel's pharmaceutical Dosage Forms and Drug Delivery Systems, 8th edition, 2004; 260-268.
2. Aulton M. The science of dosage form design, international student edition, published by Churchill Livingstone, 2002; 304-321, 347-668.
3. Banker G.S. Modern pharmaceuticals, 3rd edition Marcel Dekker Inc, New York. 576-820.
4. Bramhankar D.M. Jaiswal S.B. Controlled release medications. In: Biopharmaceutics and Pharmacokinetics treatise, 1995; 335-375.
5. Chien Y.W. Controlled and modulated-release drug delivery systems, 1995; 281-313.
6. Donald L. Handbook of pharmaceutical controlled release technology, 2002; 466-471, 738-739.
7. Durgacharan A Bhagwat., Pravin S Kawtikwar., Dinesh M Sakarkar. "Formulation and the in-vitro and biopharmaceutical evaluation of sustained release tablet of verapamil HCL using precirrol ATO5 through melt granulation technique." 2009; 278-285.
8. Government of India Ministry of Health and Family Welfare., 1999. The Pharmacopoeia of India. Delhi, India, Controller of Publication. 312-314.
9. Higuchi T. 1963. "Mechanism of sustained action medication, theoretical analysis of rate of release of solid drugs dispersed in solid matrices." J Pharm Sci. 52: 1145-1149.
10. Kuchekar., "Indian journal of pharmaceutical education." 2nd edition. 2001; 150-152
11. Lachman L., The Theory of practice of Industrial pharmacy, 3rd edition, published by Lea & Febiger, 1986; 293-345, 346-373.
12. Raymond C Rowe., Paul J Sheskey & Sian C Owen., Handbook of Pharmaceutical Excipients, 6th edition, 2009; 622-624.
13. Raymond C Rowe., Paul J Sheskey & Sian C Owen., Handbook of Pharmaceutical Excipients, 6th edition, 2009; 129-133.
14. Raymond C Rowe., Paul J Sheskey & Sian C Owen. Handbook of Pharmaceutical Excipients, 6th edition; 2009; 581-585.
15. Raymond C Rowe., Paul J Sheskey & Sian C Owen., Handbook of Pharmaceutical Excipients, 6th edition, 2009; 326-329.
16. Raymond C Rowe., Paul J Sheskey & Sian C Owen., Handbook of Pharmaceutical Excipients, 6th edition, 2009; 404-407.
17. Remington J. The science and practice of pharmacy, 21st Edition, published by Lippincott Williams & Wilkins, 2005(1); 941-948.
18. González Martín, C. González Pérez, M.A. Blanco López., "Polarographic determination of cinitapride and cinitapride". Analytica Chimica Acta, 1998(368), Issues 1-2, 175-18.
19. M.I. Colado, M.J. Alfaro, V.L. del Val, M.I. Martín., "Effect of cinitapride in isolated ileum obtained from guinea-pigs treated with morphine". General Pharmacology: The Vascular System, 1991 (5), 863-866.
20. Chiner E, Sancho-Chust JN, Llombart M, Camarasa A, Senent C, Mediero G, Gómez-Merino E., "Sleep-related painful erection in a 50-year-old man successfully treated with cinitapride". J Sex Med, 2010(11); 89-92.
21. Portinca P, Mearin F, Robert M, Plazas MJ, Mas M, Heras J., "Efficacy and tolerability of cinitapride in the treatment of functional dyspepsia and delayed gastric emptying". Gastroenterol Hepatol, 2009; 32(10); 69-76.
22. Robert M, Salvà M, Segarra R, Pavesi M, Esbri R, Roberts D, Golor G., "The prokinetic cinitapride has no clinically relevant pharmacokinetic interaction and effect on QT during coadministration with ketoconazole". Drug Metab Dispos, 2007 35(7): 49-56.
23. MILL, R. D. Asian Journal of Phytomedicine and Clinical Research.
24. Alarcón de la Lastra C, La Casa C, Martín MJ, Motilva V., "Effects of cinitapride on gastric ulceration and secretion in rats". Inflamm Res, 1998; 47(3), 131-136.
25. Alarcón-de-la-Lastra Romero C, López A, Martín MJ, la Casa C, Motilva V., "Cinitapride protects against ethanol-induced gastric mucosal injury in rats: role of 5-hydroxy tryptamine, prostaglandins and sulfhydryl compounds". Pharmacology, 1997; 54(4): 193-202.
26. Mora F, Añón R, Liceras V, Moreno-Osset E, Mínguez M, Benages A., "Metoclopramide versus cinitapride in the treatment of functional dyspepsia". A Med Interna, 1993; 10(7): 23-26.
27. Gallego Santos J, Fombuena Filpo J, Martínez López J., "Efficacy and tolerance of cinitapride on the disturbances of gastrointestinal transit". Rev Med Univ Navarra, 1991; 36(3): 12-18.

28. Colado MI, Alfaro MJ, del Val VL, Martín MI., "Effect of cinitapride in isolated ileum obtained from guinea-pig treated with morphine". *Gen Pharmacol* 1991;22(5):63-66.
29. Monés J, Espinós JC, Carrió I, Calabuig R, Vilardell F., "Gastric emptying in reflux esophagitis. Effect of metoclopramide and cinitapride". *Med Clin*, 1989;93(9):31-34.
30. Massingham R, Bou J, Roberts DJ. "A comparison of the stimulatory effects of metoclopramide and cinitapride in the guinea-pig isolated ileum". *J Auton Pharmacol*, 19855(1):41-53.
31. Gilber S, Banker and Christopher T. Rhodes, *Drugs and the Pharmaceutical Sciences*, Remington, the Science and Practice of Pharmacy, 21st Edition, 2005(8);132-157.
32. Alfred Goodman Gilman, Theodore W. Rall, Alan S. Nies, Palmer Taylor, *The Pharmacological Basis of Therapeutics*, 8th Edition, 2002(9);546-608.
33. *British Pharmacopoeia*, Department of Health, Scottish Home, and Health Department, 2008; 465-698.